

WIRELESS-CONTROLLED BIDIRECTIONAL PUMPING SYSTEM FOR ARTIFICIAL ORGANS WITH HYDRAULIC ACTUATION

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Introduction

Hydraulic soft actuation is often adopted to activate implantable systems like artificial organs, thanks to its intrinsic safety, versatility and power efficiency [1], [2]. However, the associated flow control systems proposed up to now are still far from being implantable, lacking miniaturization, powering from an on-board battery and/or wireless communication with the user [3], [4]. In this work, we introduce a portable, standalone and low-power bidirectional pumping system dedicated to implantable soft robots. A preliminary validation with an artificial urinary bladder is also presented.

Methods

The device consists of three functional blocks (Fig. 1a): an electrohydraulic switch, the electronic circuit and a battery. The switch includes a small DC pump (M200M, TCS Micropumps, UK) and a small DC motor (1512U003SR 324:1, Faulhaber, Germany) connected to a custom camshaft. This can compress four soft tubes (Fig. 1b), allowing thus fluid flow between a reservoir and the soft actuator(s) in both directions, as well as passive flow blocking (retaining the actuators' pressure, p). As such, the switch can act at the same time as a set of valves and as a bidirectional pump, by including only two active components. The electronic circuit includes an Arduino Nano 33 BLE controller, which (i) activates the pump and the motor via a driver (DRV8833, Texas Instruments, US), (ii) stops the flow at a preset p threshold by measuring $p(t)$ with a digital sensor, and (iii) interacts with a phone app via Bluetooth, receiving commands and providing feedback. A small lithium battery (3.1 Wh, 3.7 V) powers the device.

The performances of the electrohydraulic switch, in terms of flow blocking and tubes' p retention by the custom camshaft, were tested by externally pressurizing each one of the four occluded soft tubes with a minimal flow rate (1 mL/min), up to 30 kPa (i.e. twice the pump's maximum p of 15.5 kPa), and recording the $p(t)$ trend with an external sensor. The device was then employed

to actuate a detrusor muscle in an artificial bladder [4] (Fig. 1c). In four voiding tests, the Voiding Efficiency (VE: the % of output water) and the Actuation Time (AT: time to reach the set p threshold of 15.5 kPa in the actuators and switch to block mode) were measured.

Results

The occluded soft tubes showed a linear $p(t)$ increase during their pressurization, indicating no appreciable losses, and a contained p loss (mean of -2.2% from 30 kPa) in the first minute after stopping the flow. The mean VE of the artificial bladder system was 83.6%; this is comparable to the previous work from the authors [4], where the control module was bulkier (140 x 90 x 70 mm vs. 106 x 47 x 36 mm). The mean AT was 38 s (although the total VE was obtained with further pump reactivations, until injecting ~ 40 mL per actuator).

Each switch of flow mode, realized by a 90° rotation of the shaft, consumes ~ 190 mJ = 53 μ Wh (~ 255 mW for 0.75 s); each actuator filling in the above example, ~ 26.7 mWh (~ 2.53 W for 38 s); in idle mode, the board consumes 12.3 mW (mostly due to the BLE module). The circuit in [4] required instead ~ 4 W while pumping, and ~ 150 mW when idle. In the artificial detrusor case, assuming seven two-way pumping acts (i.e. urinations) of 4 min overall per day, the battery would last 48 hours.

Discussion

Thanks to its reduced size, its low power usage, and its wireless-based design, the proposed device marks the first step towards the feasible implementation of fully implantable hydraulic soft robotic systems.

References

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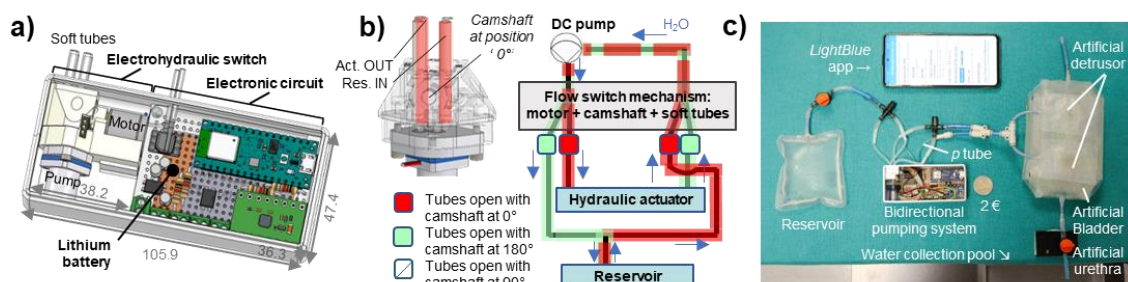


Figure 1: The bidirectional pumping system for implantable applications. a) Design overview. The whole device weights 120 g. b) Concept of the electro-hydraulic switch. c) Device application to support an active artificial urinary bladder.

